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Nanofibres In Drug Delivery System: An Overview.

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ABSTRACT

Through the ages, scientists have been developing solutions to fabricating medicine for better therapeutic activity. Nanofibres (NFs) are polymer-based, having a higher surface area to volume ratio and diameter of less than 1000nm, and 3Dtopography, porosity, and adaptable surface functions. NFs are derived from the nanomaterials to enhance bioavailability and release drugs to target sites with less toxicity. Microorganism causes infection like fungi, bacteria, etc. NF can be prepared by electrospinning, centrifuge spinning, phase separation, solution and melt blown, self-assembly, and pressurized gyration methods. The electrospinning process is most commonly used to produce a wide variety of NFs, and easy to fabricate NFs. they are monoaxial electrospinning, co-axial electrospinning, triaxial electrospinning, side by side electrospinning. NFs are of different types and they are blended NFs, core shell NFs, hallow NFs, chitosan NFs, porous NFs, NFs carbon, based on drug release mechanism, structure, and content. Degradable polymers are commonly used to modify the release of drugs. Cumulative, this review has illuminated the importance of NFs in medicine developing with various kinetics of drug release. These having antibacterial drug loaded NFs functions are wound healing, tissue engineering, and cosmetics, diagnostics, filtration and hydrogels. It regulate infectious disease, gastrointestinal tract associated disease, pain treatment, contraception and cardiovascular disorders.

Keywords: NFs, drug release kinetics, electrospinning and techniques, polymers.

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INTRODUCTION

NFs are nanomaterials with diameters that range from 1 to 1000nm. They have a high surface area to volume ratio innovative physicochemical properties and reduced porosity. A wide dispersion of containing polymers like gelatin, chitosan, Carboxy methyl cellulose (CMC), collagen, and Polyvinyl alcohol (PVC) are acceptable materials for the production and growth of NFs [1]. NFs protect the drug from decomposition before reaching the target site. Drug-loaded NFs extend drug release to produce biphasic, pulsatile, or pH-dependent drug release. Properties of NFs include enhancement of mechanical strength, increased porosity, and permeability [2]. Conventional dosage forms like capsules, tablets, and granules, and drugs given via parenteral routes have diverse drawbacks such as first-pass metabolism which can be overcome by using NFs [3].

NFs types

Blended NF

Blended NFs are produced from single-phase material structures. Two fibers are composed of one structure consisting single or a combination of materials, their active component to achieve a pharmacokinetic profile. A suitable methodology for incorporating active ingredients needs to be developed based on the characteristics of the drug. As reported by Nakielski et al polymer solution was formulated by dissolving poly-L-lactic acid in a 9.1(w/w) mixture of N, N-dimethylformamide, and CHCl_3 . Kim et al successfully synthesized hyperthermia NFs by utilizing an electrospinning technique to initiate pharmacokinetic release for inducing tumor self-destruction.

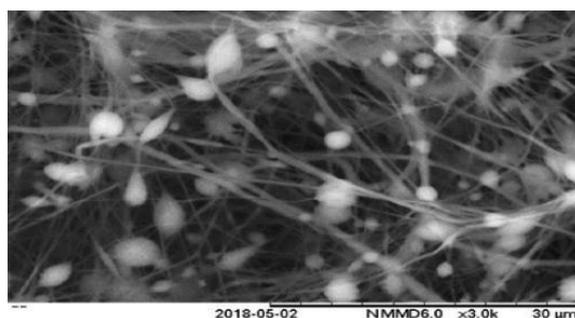


Figure 1: Blended NF

Core-shell NFs

A core-shell NF configuration is applicable whenever medicine containing NFs is possibly inactivated *in vivo* before initiation to timely performance [4]. The core fiber containing medicine in this methodology shields it from harsh *in vivo* conditions until therapeutic action is required. Recently, core-shell NFs have been fabricated to import diverse active molecules like medicine, genes, and proteins for their prolonged release. It is mainly used to avoid the burst release [5].

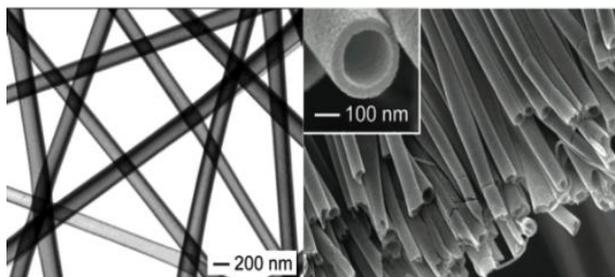


Figure 2: Core-Shell NFs

Hallow NFs

Hallow NFs are used in the storage of hydrogen and nanofluidics. These are prepared by methods like co-axial spinning and chemical vapor deposition. These fibers are filled with substances like poly and caprolactone, with polyethylene glycol as the core substance [6]. They are mostly applicable in gas sensing [7]. metal oxide NFsexhibits unique properties due to their morphology, physical and chemical properties. Specifically, the structure provides distinct electrochemical, catalyst, and electrical properties [8].

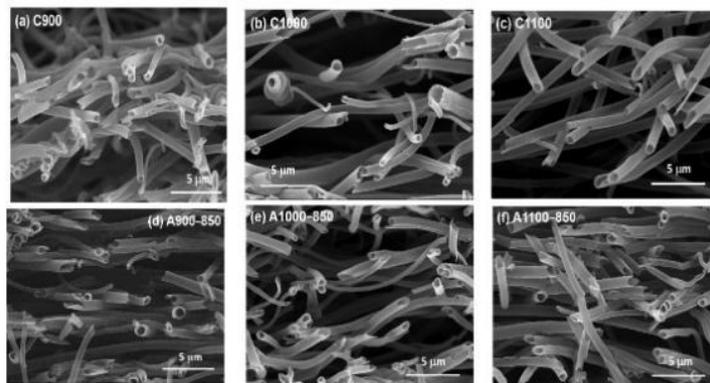


Figure 3: Hallow NFs

Chitosan NF

Living organisms produce chitin, the second most prevalent naturally occurring polysaccharide. Chitosan and chitin are hydrating, bio-compatible, nontoxic, biodegradable, anti-microbial agents, and readily form gels. These NFs are used to air filter media for water purification [9]. Chitin is deacetylated to prepare chitosan NF. Chitin is insoluble in water and precipitates. Their NFs distribute uniformly, and as a result, the dispersion is readily processable and shape able [10].

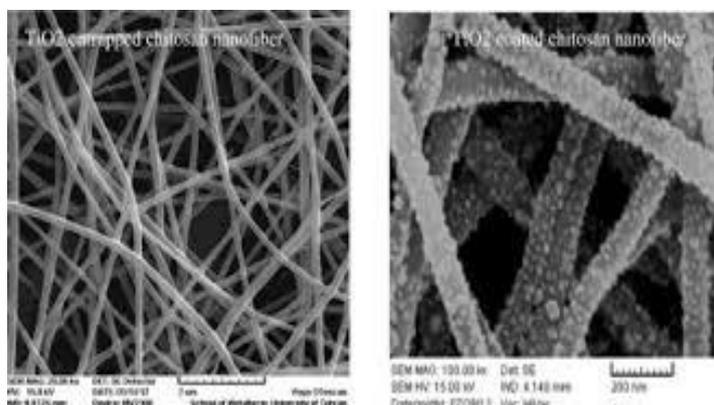


Figure 4: Chitosan NF

Porous NFs

Because of the high surface area of porous used in a fuel cell, filtration, catalysis, and drug delivery. Porous is produced by using particular polymeric solvent mixtures under controlled conditions [11]. the structure of porous increases surface area along with capacity of adsorption and acts as diffusion channel to offer reaction sites and transfer substance [12].

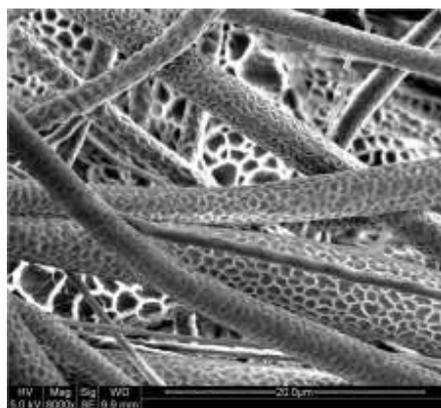


Figure 5: Porous NFs

NFs carbon

Graphitic NFs having many properties using carbon-containing gases and metallic catalysts. Rapid expansion of thin fibers results in weak particles, and slower expansion of thick fibers results in strong particles. Carbon NFs use in catalyst support materials [13].

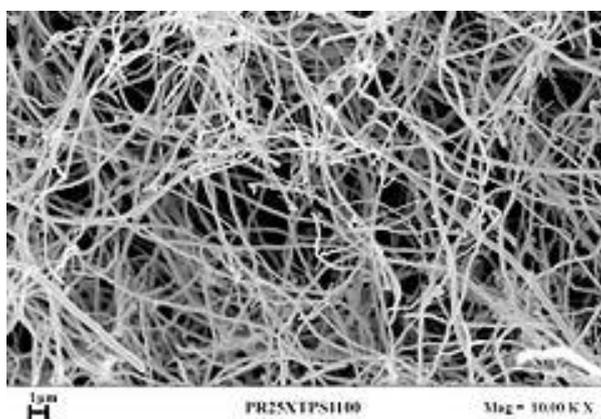


Figure 6: NFsCarbon

TECHNIQUES

Electrospinning

Electrospinning is a highly adaptable and reliable method to produce with controlled surface topography. In this process, fine-charged jets are produced by the application of a strong electric field to liquids like polymer solutions, suspensions, and emulsions containing pharmaceutical ingredients [14]. Polymers used in electrospinning are silk fibroin, chitosan, collagen, and gelatin hyaluronic acid.

Parameters influencing the electrospinning process

FACTOR	PARAMETER	EFFECT ON FIBRE
Process	<ul style="list-style-type: none"> • Voltage • Flow rate • The small distance between the collector and the needle 	<ul style="list-style-type: none"> • Decrease in diameter due to increase in voltage. • Increase diameter due to increase in flow rate. • Increase diameter due to the small distance between collector and needle
Solution	<ul style="list-style-type: none"> • Polymer concentration • Viscosity 	<ul style="list-style-type: none"> • Increase in diameter due to increase in polymer concentration

		<ul style="list-style-type: none"> • Increase in diameter due to increase in viscosity
Environmental	<ul style="list-style-type: none"> • Temperature 	<ul style="list-style-type: none"> • Decrease in diameter due to increase in temperature.

Types Of Electrospinning

Monoaxial Electrospinning

It is a commonly used method. Its setup comprises of high voltage power a syringe container with individual blunt metallic needles and electrode collector located at a controlled distance from the oppositely polarized needle, vertically or horizontally first the polymer solution is loaded into a syringe separated at standardized velocity using a syringe pump generating liquid hemisphere droplet at the tip of spinneret electrostatic charges accumulate at the surface of the droplet as result of the voltage applied on needle. When the electric field is outgross the specific value, the electrostatic forces conquer the surface tension of the polymer solution, catalyzing the formation of a Taylor cone from the liquid droplet. Due to electrohydrodynamic stress setting process occurs in working distance. This leads to solvent evaporation and deposition on the collector [15].

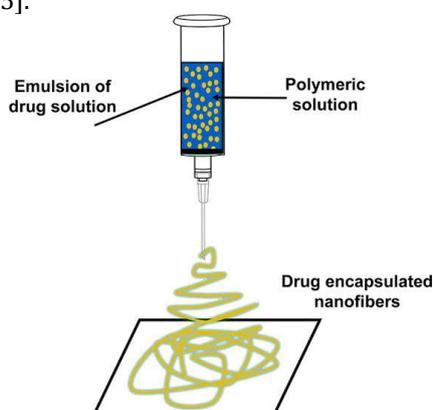


Figure 7: Monoaxial Electrospinning

Co-Axial Electrospinning

Co-axial electrospinning utilizes the sheath solution to produce hollow and functional fibers which may contain coating. During this process, spinners with immiscible polymeric solutions operate at multiple flow rates from the single needles part [16]. The shell solutions circulate the spinneret holding core solution to the spinneret tip up to the solution connect and attract towards the collector as a result of utilized electrostatic potential difference. The structure of the core-shell is maintained throughout the entire procedure, this leads to the formation of core-shell fibrous by utilizing co-axial electrospinning in single core-sheath fibers multiple drugs can be loaded and control the drug release kinetics [17].

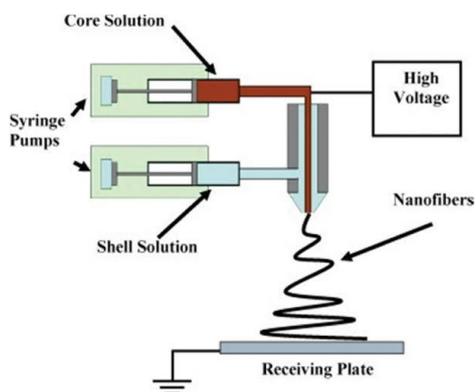


Figure 8: CO-Axial Electrospinning

Triaxial Electrospinning

Three layered fibers are produced by triaxial electro-spinning layers core, intermediate, and shell layer. Triaxial electrospinning consists spinneret fluid-driven pump, collector, and high-voltage generator with three concentric needles through three different pumps three polymer solutions are transferred near the spinneret apex throughout the Triaxial electrospinning. The solution deformed into a Taylor cone under the influence of electrostatic force. During bending, the instability experienced by the jet leads to solvent evaporation, dry fiber is deposited on the collector wall [18].

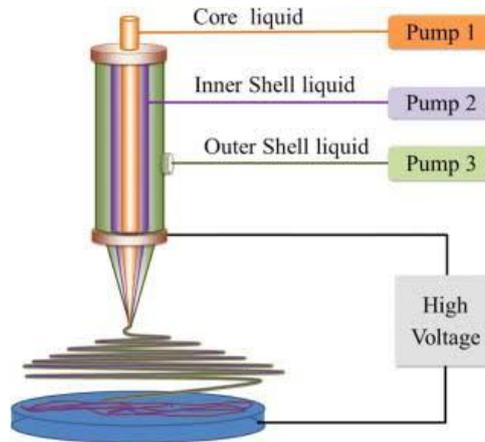


Figure 9: Triaxial Electrospinning

Side-by-side electrospinning

Through nozzles arranged side by side 2 separate polymer solutions are delivered but capillaries up are attached to a high voltage supply the polymer solution remains separate until reaching the capillaries end throughout the process, as solute near the tip of the capillary, from the nonuniform solution mixture Taylor cone is produced. These fibers deposit on collector after evaporation of the solvent in this electrospinning, both polymer solution must have the same conductivity to produce a single Taylor cone.

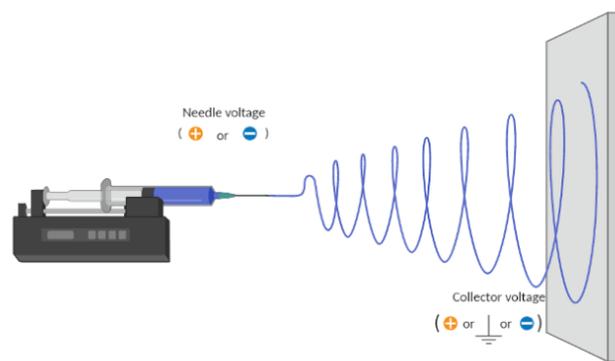


Figure 10: Side-by-side electrospinning

Centrifugal spinning

Centrifugal spinning is also called as rotary spinning (or) rotary jet. In this process, polymer solution and emulsions are mixed to develop fibers and are mainly used for the production of glass wool (or) fiberglass. Fiberio Technology Corporation has beneficially standardized a centrifugal spinning method for industrial-scale production [19].

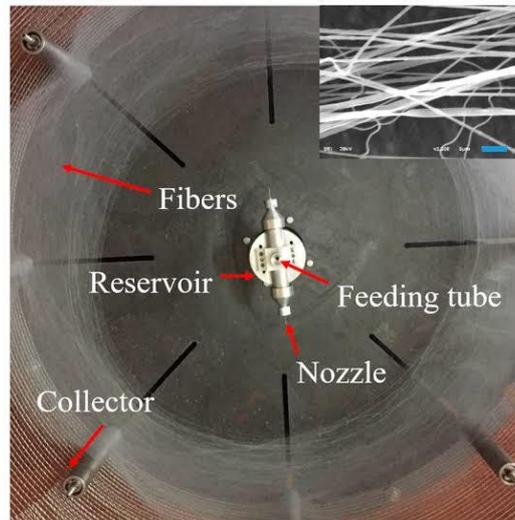


Figure 11: Centrifugal spinning

The mechanism of centrifugal spinning is shown in Fig (11), In the centrifugal spinning process, the liquid solution is poured into a spinning rotating head, which includes multiple nozzles around the the sidewall. If increase in rotation speed at a critical value, centrifugal force exceeds the surface tension of spinning fluids, and the jet of the solution is released from the nozzle, the solvent is prolonged through the liquid jet, which evaporates concurrently, up to result in the collector wall in the fibers form. It is a pressurized gyration. It can be evaluated as pressure-assisted centrifugal spinning. Centrifugal spinning is a different method for producing with well-defined structure at high speed and less cost. It can be divided into two, they are nozzle and nozzleless type. The important parts of centrifugal spinning include the spinning head and motor [20].

Centrifugal spinning main forces:

Centrifugal spun jet is difficult due to the rotating spinning head, while it is used to study the forces loading on a jet to compute the conditions of optimal spinning. In centrifugal spinning, there are two main forces to prolong the jet, the viscous force and the centrifugal force. The centrifugal spinning is the applicable dimension of the spinning head and rotational speed. Viscous force applies to the concentration of solution and polymer molecular weight. The centrifugal spinning is double larger than electrospinning. Concentration is high, which means the solvent is less used, which is an advantage of centrifugal spinning.

Centrifugal Force = According to the Equation of

$$F = mrw^2$$

- F = Centrifugal Force
- m = weight of spinning dope
- r = radius
- w = angular speed

Factors affecting centrifugal spinning

FACTORS	PARAMETERS	EFFECT ON FIBRE
Solution	<ul style="list-style-type: none"> • Surface tension • Viscoelastic 	<ul style="list-style-type: none"> • Production of bead fibers due to a decrease in surface tension • Beads formation occurs at low viscosity.

<p>Processing</p>	<ul style="list-style-type: none"> • Rate of solvent evaporation • Centrifugal force • Orifice radius • Spinneret angular velocity 	<ul style="list-style-type: none"> • A low rate of solvent evaporation leads to the formation of thin film fibers. • Formation of beads occurs at a higher centrifugal force. • Decrease in fiber diameter with a decrease in the diameter of the orifice and fewer beads. • Beads on fibers occur at lower angular velocity.
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Solution and melt-blowing spinning

The melt blown has top priority amongst nonwoven methodologies for the production of NFs. In this method through fine capillary the molten polymer is pumped across the capillary and formed into fibers, regulated by hot gas flow with high velocity exiting coaxially polymer melt. These fibers are deposited on the screen and form a nonwoven web [21]. In this method, polymers like polyamide, polyester, etc. currently solution blowing come into practice, where extrusion of polymer solution occurs not polymer melt producing solution blowing spinning fiber depends upon polymers molecular weight, viscosity, and concentration of polymer solution and flow rate of polymer solution [22].

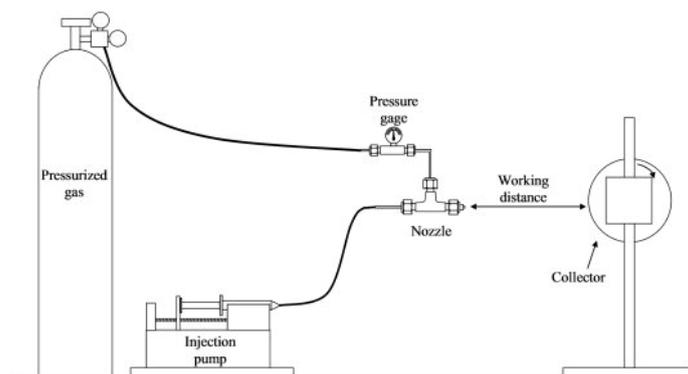


Figure 12: Solution and melt-blowing spinning

Parameters influencing the solution and melt blown

Parameter	Factors	Effect
<p>Process</p>	<ul style="list-style-type: none"> • Flow rate solution • Air pressure 	<ul style="list-style-type: none"> • Measure the diameter of fiber with an increase in flow rate solution. • Droplets will form on fiber with a decrease in air pressure.
<p>Solution</p>	<ul style="list-style-type: none"> • Viscosity • Molecular weight • Surface tension 	<ul style="list-style-type: none"> • Increase in viscosity increase in diameter • Increase in molecular weight leads to the formation of beads. • Increase in surface tension leads to the formation of beads

Ambient condition	<ul style="list-style-type: none"> • Temperature • Humidity 	<ul style="list-style-type: none"> • Increase in temperature leads to a decrease in the diameter of the fiber. • Increase in humidity small pores will form.
System	Diameter	Decrease in diameter of fiber with decrease in of nozzle.

Pressurised gyration

This is a strategy for forming polymer fibres, that combines solution blowing and centrifugal spinning. Pressurized gyration apparatus affects the instability of polymer solution due to the interaction of daylength-taylor interaction. The polymer solution is shifted because of increasing centrifugal force as the vessel spins. The gas pressure is applied, liquid is pushed out of the vessel. On a concentrated Polymer jet, a liquid air surface tension gradient is produced [23]. this gradient furtherly causes marangonic stress right angle to the liquid-gas interface that activates the movement of polymer droplets, once the evaporation of solvent occurs, the fiber is produced from the extruded polymer in the jet. The formation of fibers depends upon process, solution, system, and ambient parameters [24].

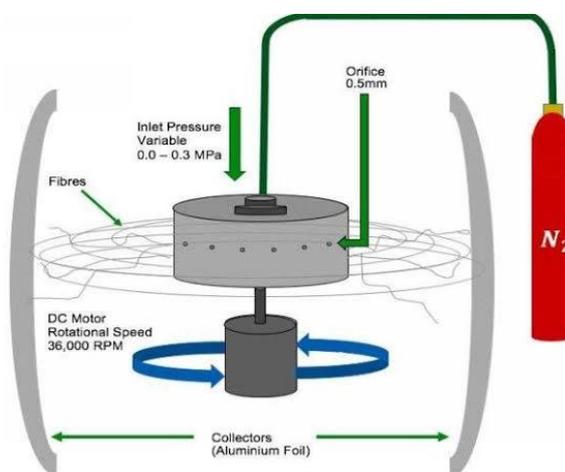


Figure 13: Pressurized Gyration

Parameters influencing the pressurized gyration process

Parameter	Factors	Effect
Process	<ul style="list-style-type: none"> • Working pressure • Spinneret rotating speed 	<ul style="list-style-type: none"> • An increase in working pressure decreases the diameter of fibers. • An increase in spinneret rotating speed decreases the diameter of fibers.
System	<ul style="list-style-type: none"> • Orifice 	<ul style="list-style-type: none"> • Increase in size of orifice increase in diameter of fibre
Solution	<ul style="list-style-type: none"> • Polymer concentration • Volatility of solvent 	<ul style="list-style-type: none"> • Increase in polymer concentration increase in diameter of fiber • Increase in volatility decrease the diameter of fiber
Ambient	<ul style="list-style-type: none"> • Temperature • Relative humidity 	<ul style="list-style-type: none"> • No direct effect • An increase in relative humidity causes decrease in the uniformity of fiber.

Applications of NFsin drug delivery system

Cardiovascular diseases: the NF contains stem cells that can cure cardiovascular diseases like atherosclerosis and cardiomyocyte regeneration [25].

Wound dressing: skin can heal itself, open skin wounds infected by microorganisms cause infection. And spread nearby healthy tissues and wound healing is delayed. The therapeutic material for this is wound dressing but it can't meet all requirements like strongest hemostasis, non-adherence to wounds, nontoxic, etc in recent days, polymer with specific shapes similar to the extracellular matrix, allowing the supporting all protection and healing damaged cells [26].

In cancer therapy: cancer is abnormal cell growth that invades surrounding tissues and organs. To treat cancer chemotherapy which kills cancer cells along with stem cells in our body. To overcome this are used for targeted delivery [27].

Dentistry: A variety of microbial species causes oral infections. To treat these infections with no cytotoxicity NFs are used in recent years. Nano dentistry is a combination of oral health with nanotechnology for the treatment, prevention, and diagnosis of the health of dental [28].

Cosmetics: are also used in cosmetics for skin such as cleansing, and healing, NF releases the ingredients for a longer time that shows beneficial effects. For example: in the cosmetic field, they deliver various types of vitamins to the skin.

Transdermal drug delivery: NFs are used for transdermal drug delivery to overcome the challenges. Due to their low toxicity, biocompatibility, favorable features, and biodegradability, NFs are used [29].

Other applications

- Drugs are protected from the harsh biological environment from NFs.
- The NFs release the drug in small portions in two hours initially, protecting the stomach membrane, and aspirin release is extended with no cytotoxicity.
- Nano fibers loaded with progesterone hormone to offer controlled drug delivery.
- Nano fibers loaded with cinnamon to provide antifungal activity.

CONCLUSION

In this review, we have discussed the development using various techniques. The types of NF are hollow NF, carbon fiber, chitosan NF, blended NF, core-shell NF, porous NF, and their properties. Specific applications of each type of NF are mentioned. We have also discussed the different techniques like electrospinning, centrifugal spinning, solution and melt-blown spinning, and pressurized gyration. Electrospinning is the most important technique to produce NF. The monoaxial electrospinning, coaxial electrospinning, triaxial electrospinning, and side-by-side electrospinning are discussed. Coaxial electrospinning can produce materials with multiple functions. Monoaxial electrospinning produces extended drug-release NFs. Triaxial spinning produces complicated NFs, and side-by-side spinning is used to produce Janus fibers. Centrifugal spinning is utilized to produce glass fibers. Pressurized gyration is a combination of centrifugal spinning and solution and melt-blowing spinning. Overall, this review illustrated the importance, poly valence, of NFs in various drug delivery systems like cosmetics, cardiovascular disease, etc, with their drug release kinetics. Therefore, drug release profiles for all specific drug delivery systems are consistently built to order even though the use of NFsin drug delivery has shown significant potential for obtaining specific drug releases, later more studies are needed to illustrate their clinical and commercial applications.

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